

## MODELING FLOWS IN COLLAPSIBLE TUBES

**Xiaoyu Luo**

*University of Glasgow, UK*

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### Summary

This chapter summarizes some recent modeling work of flows in flexible or collapsible vessels, with particular focus on a prototype problem concerning self-excited oscillations in the Starling Resistor. Although self-excited oscillations in collapsible tube flows have been extensively studied, our understanding of their origins and mechanisms is still far from complete. The paper starts briefly with the background to the problem, and introduces some mathematical and numerical approaches based on one-dimensional, two-dimensional, and three-dimensional models. The summary is not intended to be exhaustive but is designed to offer a flavor of the research in this area, and is inevitably focused on the work familiar to this author.

### 1. Introduction

In physiological fluid mechanics, blood flow inside large vessels may collapse and experience interesting self-excited oscillations under a negative transmural (internal minus external) pressure. These vessels are thus collapsible tubes. Flows in collapsible tubes form a significant branch of the biological and physiological applications of internal flow. Veins above the level of the heart can collapse as the transmural pressure  $P_{tm}$  reduces as external muscles squeeze (Wild et al, 1977, Pedley, 1980). Intramyocardial coronary blood arteries collapse during heart contraction in systole (Guiot et al., 1990). Similar behavior is seen in the branchial arteries compressed by a sphygmomanometer cuff (Bertram and Ribreau, 1989), in the large airways during forced expiration (Shapiro, 1977, Kamm and Pedley, 1989), and in the urethra during micturition (Griffiths 1989).

These, and the closely related problems, have been studied by various research groups

over the last 40 years, ranging from flow in giraffe jugular vein to peristaltic pumping, and to flow over compliant surfaces (Shapiro, 1977, Brook and Pedley, 2002, Ku, 1997, Elad et al., 1989, Dia et al., 1999, Tang et al., 1999, Tutty and Pedley, 1993, Elad et al., 1987, Gavriely et al., 1982, Kamm and Shapiro, 1979, Davies and Carpenter, 1997, Cancelli and Pedley, 1985, Carpenter and Pedley 2003, Carew and Pedley, 1997, Jensen, 1990, Rast, 1994, Luo and Pedley, 1996, Grotberg and Gavriely, 1989, Hazel and Heil, 2003, Heil and Pedley, 1995, Guneratne and Pedley, 2006), to mention just a few. Some earlier reviews are given by Kamm and Pedley (1989), Pedley and Luo (1998), Bertram (2004), and Grotberg and Jensen (2004).

In this chapter, we shall limit our attention to studies that form a sub-set of applications concerning the flow in large vessels, focusing on the phenomena observed from the Starling Resistor.

## 2. The Starling Resistor and the Tube Law

The Starling resistor is a commonly used bench-top apparatus for studying flow in collapsible tubes, as depicted in Figure 1.

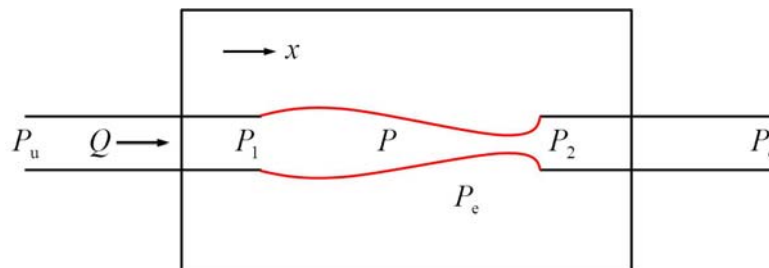


Figure 1. Sketch of a Starling resistor.  $p_1$ ,  $Q$  are pressure and flow rate upstream of the collapsible segment;  $p_e$  is the external pressure,  $p_2$  is the pressure downstream,  $p_u$  is the total pressure far upstream and  $p_d$  is the pressure far downstream. In the absence of the upstream and downstream tube resistances,  $p_1 = p_u$ , and  $p_2 = p_d$ .

It was first used in a study of cardiac functions by Knowlton and Starling (1912) to predict the collapse of a tube. The apparatus consists of a collapsible rubber tube fixed at both ends inside a chamber where the external pressure  $p_e$  can be adjusted independently. Fluid is held upstream in a reservoir from which it passes through a rigid tube into the collapsible segment in the chamber and out into a downstream reservoir. Resistors downstream are in place to control pressure and flow at the entrance and exit of the collapsible segment. When flow is driven through the elastic tube section, the transmural pressure,  $p - p_e$ , can become sufficiently negative due to the Bernoulli effect, that the tube collapses, partially or fully, with reduced cross-sectional area  $A$ . The relationship between  $p - p_e$  and  $A$  is known as the "Tube law".

Unlike fluid flowing through a rigid tube, here more combinations of control parameters are possible. For example, one may specify the pressure head ( $p_1 - p_2$ ), or flow rate

$Q$ , while keeping downstream transmural pressure  $p_2 - p_e$  constant. These are sometimes referred to as the “pressure-driven system”, or “flow-driven system”, respectively (Liu et al., 2012). Alternatively, one can study the pressure- or flow-driven systems while keeping the upstream transmural pressure  $p_1 - p_e$  fixed. Each of these settings determines a specific system with its own unique characteristics. The commonly observed “flow limitation” (Gavriely et al., 1989) and “pressure-drop limitation” (Bertram and Castles, 1999), are interesting phenomena corresponding to specific configurations of these settings. If we increase  $p_1 - p_2$  while keeping  $p_1 - p_e$  constant, then at some point the flow rate cannot be increased further, and this is called “flow limitation”. Likewise, if we increase  $Q$  while keeping  $p_2 - p_e$  constant, then soon or later the pressure-drop will stop increasing; this is “pressure-drop limitation”. In fact, pressure-drop limitation can even show up as “negative effort dependence”, whereby the flow rate increase is accompanied by pressure drop decrease (Gavriely et al., 1984, Gavriely and Grotberg, 1988, Luo and Pedley, 2000).

Over the last 30 years, Bertram and co-workers have conducted a sequence of extensive experimental studies of this system (Bertram, 1980, 1995, Bertram and Castles, 1999, Bertram and Chen, 2000, Bertram and Elliott, 2003, Bertram et al., 2001, Bertram and Tscherry, 2006). One of the interesting phenomena observed in these experiments is self-excited oscillation, when a spontaneous fluctuation in pressure, flow and cross-sectional area of the tube occurs (Conrad, 1969, Bertram, 1986, Low et al., 1997). It is important to recognize that pressure drop may not be the only contributing factor involved in the collapse. The length and rigidity of the tube also play a significant effect on collapse and subsequent self-excited oscillations (Bertram, 1980).

Despite the seemingly straightforward experimental setup, the nature of the self-excited oscillations was proven to be rather difficult to explain. However, over the years, there have been some significant advances in the analytical and simulations. In the following, we provide a brief summary of the progress made to date, which ranges from early lumped parameter models to fully three dimensional simulations, with particular attention to several recent approaches developed by this and other groups in the last few years. Some of the earliest developments were lumped parameter, or zero-dimensional models such as (Conrad, 1969, Shapiro, 1977, Bertram and Pedley, 1983) which focused on describing pressure and flow as function of cross-sectional area only, at the narrowest point. This simplification enables one to obtain a 2nd or 3rd order ODEs, depending on inlet boundary conditions. These models can be used successfully to produce some self-excited oscillations. The models highlight the importance of energy dissipation in order to sustain the self-excited oscillations, and show that the flow-driven system (which can be described by 2nd order ODE) is more stable than the pressure-driven system (which is often described by 3rd order ODE). However, in general these models cannot incorporate many real mechanical features. Their inability to capture wave propagation is a fundamental limitation which prompts the development of 1D models.

### 3. One-Dimensional Models

A simple one-dimensional model for a steady flow is described by Shapiro (1997)

$$\frac{d}{dx}(uA) = 0, \quad (1)$$

$$u \frac{du}{dx} = -\frac{1}{\rho} \frac{dp}{dx} - R(A, u)u, \quad (2)$$

$$p - p_e = P(A), \quad (3)$$

where  $A$  is the cross-sectional area,  $u$  is the velocity,  $p$  is the pressure,  $x$  is the longitudinal coordinate,  $Ru$  ( $R > 0$ ) represents the resistance, and  $P(A)$  describes the tube law.

Combining (1) and (2), we have

$$\frac{dA}{dx} = -\frac{RuA}{c^2 - u^2},$$

where  $c = \left(\frac{A}{\rho} \frac{dP}{dA}\right)^{1/2}$  is the speed of propagation of long, small-amplitude pressure waves.

These equations are exactly analogous to those for free-surface flow in shallow water channel. It is immediately clear that the steady model breaks down when  $u$  approaches  $c$ . This is known as "choking", analogous to a hydraulic jump in shallow water in a channel flow. A number of researchers have gone further to advocate that the fluid velocity becoming comparable to the wave speed, i.e. the occurrence of flow-limitation, is the major mechanism for the onset of self-excited oscillations. However, later experiments by Bertram and Raymond (1991) and computations by Luo and Pedley (2000) cast doubt over a causal link between choking and self-excited oscillations.

Indeed, it is now believed the "choking" mechanism is not responsible for self-excited oscillations in the Starling resistor, since the length of tube used is too short for choking to occur, and the 1-D model fails to describe the downstream (tube re-opening) conditions (Pedley and Luo, 1998).

To address this issue, a modified 1-D model was developed to include tension,  $T$ , and energy dissipation (Cancelli and Pedley, 1985, Jensen and Pedley, 1989, Luo and Pedley, 1995), with the governing equations

$$\frac{d}{dx}(uA) = 0, \quad (4)$$

$$\chi u \frac{du}{dx} = -\frac{1}{\rho} \frac{dp}{dx} - R(A, u)u, \quad (5)$$

$$p - p_e = P(A) - T \frac{d^2 A}{dx^2}, \quad (6)$$

where  $\chi$  is the dissipation constant ( $0 < \chi < 1$ ), (6) is the updated tube law, and  $P(A)$  is empirically determined.

One simple form of  $P(A)$  is (Jensen and Pedley, 1989):

$$P(A) = \begin{cases} K_p (1 - \alpha^{-3/2}) & \text{for } \alpha < 1, \\ K_p (\alpha - 1) & \text{for } \alpha > 1, \end{cases}$$

where  $\alpha = A/A_0$ , and  $K_p$  is a constant. Using this model, Jensen and Pedley (1989) showed that, as long as there is energy loss in the system i.e.  $\chi < 1$ , then a steady solution exists for all positive values of flow rate and tension  $T$ . Since energy loss is inevitable, this suggests that the breakdown of the steady flow model is not caused by choking, but must arise through the global instabilities of the steady solutions. Indeed, this has been proved by (Luo and Pedley, 1996), among others, using two-dimensional models. More advanced 1-D approaches were used by (Pedley and Luo, 1998, Stewart, 2009), based on a long wavelength assumption. In this case, the mass and momentum equations are integrated across the two-dimensional channel height  $h$ , to give

$$h_t + (Uh)_x = 0, \quad (7)$$

$$U_t + UU_x + \frac{1}{h} \left( \int_0^h u^2 dy \right)_x = -p_x + \frac{1}{hRe} [u_y]_0^h, \quad (8)$$

$$p - p_e = Th_{xx} (1 + h_x^2)^{-3/2}, \quad (9)$$

where  $T$  is the membrane tension,  $p_e$  is the (constant) external pressure,  $U$  is the average velocity across the channel,  $u$  represents the velocity fluctuation across the channel, and  $Re$  is the Reynolds number, defined as the ratio between the inertia and the viscous forces. Using the Karman-Pohlhausen approximation with a specific velocity profile, Pedley and Luo (1998) solved these equations and explored various assumptions of relating the pressure drop to flow separation downstream of the narrowest cross-sectional area. Essentially, they showed that these 1-D models cannot predict the full strength of the energy loss seen in the 2-D models when the wall deformation is severe.

On the other parameter region, in the limit of the high-Reynolds number region and when the channel deformation is small, Stewart (2009) was able to use this type of 1-D systems to capture the mode-1 “sloshing” oscillations initially identified by Jensen and Heil (2003) using an asymptotic analysis (where mode- $i$  indicates that the perturbation profile contains  $i$  humps). By further analyzing the energy budget for high-Reynolds-

number and pressure-driven systems, they showed that the energy budget behaves differently in mode-1 and mode-2 oscillations. For mode-1 oscillations about the uniform base state, the time-averaged net kinetic energy flux into the system is positive, therefore the kinetic energy is extracted from the mean flow and is dissipated by the oscillations. However, for mode-2 neutral oscillations, the time-averaged net kinetic energy flux into the system is negative, suggesting a different physical mechanism. Recently, Xu et al. (2013, 2014) considered a 1-D model under a uniform base state for a flow-driven (flux-driven) system, which is identical to the model used by Stewart et al. (2009, 2010) except for the boundary conditions. Using asymptotic analysis, they revealed that when the downstream length is comparable to the membrane length, the system becomes unstable when a Hopf and transcritical bifurcation arise simultaneously, giving rise to mode-2 perturbations (i.e. membrane displacements with two extrema). However, when the downstream length is much longer than the membrane length, there is an independent mechanism of instability that is intrinsically coupled to flow in the downstream rigid segment, and is promoted by a 1:1 resonant interaction between two modes. These studies provided new insight to the nature of self-excited oscillations that occurring in the system. However, due to the assumptions introduced, further two and three-dimensional computational studies are necessary to assess the wider relevance of the instability mechanisms identified therein.

#### 4. Two-Dimensional Models

Due to the complexity of three-dimensional models and high computational requirements, two-dimensional models are used extensively to understand the mechanisms of the rich dynamic behavior observed in the Starling Resistor system. A widely used two-dimensional approach was introduced by Pedley (1992), in which the fluid mechanics is based on a lubrication theory. This is also known as the "Fluid-membrane" model, which consists of a channel flow with two rigid parallel planes, with the upper wall replaced by a thin membrane of length  $L$ . The membrane has no bending stiffness and inertia but is under longitudinal tension  $T$ , as shown in Figure 2. This system is simpler than 3D models but in principle can be realised experimentally.

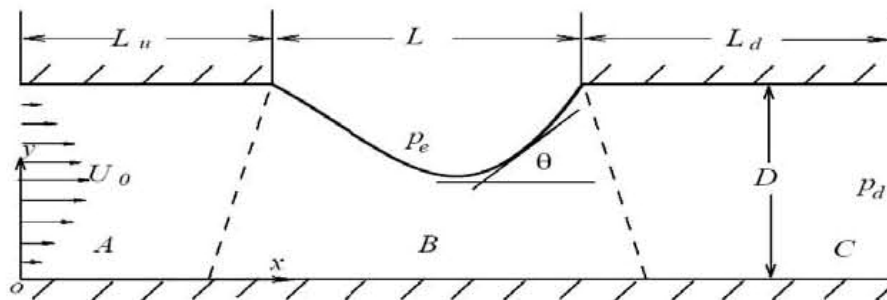


Figure 2. Sketch of the two-dimensional model.

The fluid mechanics in this model was later improved by using the Stokes equations (Lowe and Pedley, 1995), and then the Navier-Stokes equations (Luo and Pedley, 1995), so that the steady governing equations of the system are

$$\text{Re} u_{i,j} (u_j) = -p_i + u_{i,jj}, \quad (10)$$

$$u_{j,j} = 0, \quad (11)$$

$$p_e - p = \kappa T \quad (12)$$

Where  $Re$  is the Reynolds number, and the coordinates are scaled with the rigid channel height  $D$ , the velocity components  $u_i$  are scaled with the inlet velocity  $U_0$ , tension  $T$  is scaled with  $\mu U_0$ , pressure  $p$  is scaled as  $p = \bar{p}D/\mu U_0$ , and  $\kappa$  is the curvature calculated from the channel height  $h$  under the elastic section:

$$\kappa = h''(1 + h'^2)^{-3/2}.$$

These equations were solved by (Rast, 1994, Lowe and Pedley, 1995, Luo and Pedley, 1995) using the finite element methods. At the low Reynolds number, the solutions agree very well with the results using the lubrication theory, and importantly, solutions exist for almost any positive values of the membrane tension. The only limitation comes from the numerical scheme, which fails to converge if tension is too small. For a Reynolds number ( $Re$ ) of up to a few hundred, Shim and Kamm (2002), and Rast (1994) predicted steady membrane configurations similar to those of 1D models, but showed more fluid flow details, such as flow separation downstream of the collapsed section, long-wavelength nonlinear standing waves downstream of the constriction, and vortex-shedding eddies along both walls.

Treating the flexible segment as a membrane and assuming  $Re \gg 1$ , Guneratne and Pedley (2006) used interactive boundary-layer theory to describe steady flows: when the transmural pressure downstream  $\sim 0$  and the membrane tension  $T$  is reduced from an initially large value, the system exhibits an increasing number of static eigenmodes arising via a static divergence instability; nonzero values of  $p_e$  break the symmetry of the solution structure so that as  $T$  falls one passes through regions of parameter space exhibiting single, multiple, or no steady solutions.

Huang et al. (2001) assumed that the membrane has inertia, damping, and relatively low tension. This enabled him to analyze the linearized Navier-Stokes equations, and he showed that the system exhibits both static divergence (at sufficiently low tension) and flutter (dependent on the membrane inertia), which are sensitive to the choice of upstream and downstream boundary conditions.

Using the arbitrary Lagrangian-Eulerian (ALE) approach, Luo and Pedley (1996) embarked on unsteady modeling of a fully coupled nonlinear system:

$$\frac{\partial u_i}{\partial t} + u_{i,j}(u_j - u_j^A) = -p_{,i} + \frac{1}{Re}u_{i,jj}, \quad (13)$$

$$u_{j,j} = 0, \quad (14)$$

where all others variables are the same as in (10)(11) but now the pressure  $p$  in (12) is replaced by the normal stress component which is scaled with the dynamic pressure

head  $\rho U_0^2$ , and  $T$  is scaled with  $\rho U_0^2 D$ . Note  $u_j^A$  is the grid velocity which is in general non-zero. In the extreme cases when  $u_j^A = 0$  or  $u_j$ , the equations are described in the Lagrangian or Eulerian frame of reference. These are solved with a Petrov-Galerkin finite element scheme coupled with a spine method. For six-node triangle elements, it can be shown that in this approach the geometric conservation law is exactly satisfied (Liu et al., 2012). Luo and Pedley (1996) showed how these steady flows can become unstable to self-excited oscillations if  $Re$  is sufficiently high or the membrane tension sufficiently low. The membrane oscillations are found to be closely associated with the downstream propagating waves in the inviscid core flow beyond the constriction. These resemble the vorticity waves or large-amplitude TS waves described previously by Stephanoff et al. (1983), Ralph and Pedley (1988). Luo and Pedley (1996,1998) also found that the dissipation primarily occurs in the viscous boundary layers on the channel walls upstream of the constriction, and not in the downstream separated flow zones as was previously expected, which is illustrated by Figure 3.

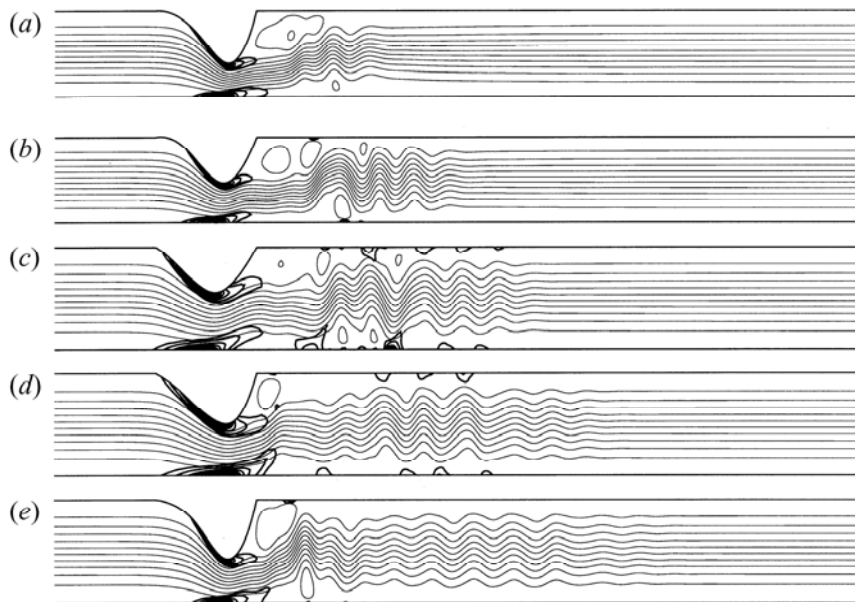


Figure 3. Snap shots of instantaneous streamlines (lighter lines) and energy dissipation contours (darker lines) generated in the self-excited oscillations by Luo and Pedley (1998).

In addition, Luo and Pedley (1998) showed how introducing inertia in the membrane allows an additional high-frequency flutter mode to grow. In a subsequent study (Luo and Pedley, 2000), they found existence of multiple solutions for a given set of control parameters, and how the primary instability is sensitive to the choice of boundary conditions. The system is more stable when the upstream flux, rather than the pressure drop, is prescribed. Using interactive boundary-layer equations, Pihler-Puzovic and Pedley (2013) discovered that for high-Reynolds-number flow in a two-dimensional collapsible tube, a unique steady solution exists when the pressure is fixed precisely at the downstream end of the membrane, but there are multiple states possible if the pressure is specified further downstream. They also found that no self-excited



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## Bibliography

### References

- C.D. Bertram. Energy-dissipation and pulse-wave attenuation in the canine carotid-artery. *Journal of biomechanics*, 13(12):1061-1073, 1980. (This paper presents methods for calculating viscous and viscoelastic energy dissipation and attenuation coefficient for a segment of artery in vivo).
- C.D. Bertram. 2 modes of instability in a thick-walled collapsible tube conveying a flow. *Journal of biomechanics*, 15(3):223-224, 1982 (This paper describes different modes of stabilities in thick-walled collapsible tube flows).
- C.D. Bertram. Unstable equilibrium behavior in collapsible tubes. *Journal of biomechanics*, 19(1):61-69, 1986. (Experimental study of thick-walled silicon rubber tube, where three types of equilibrium under a constant upstream pressure are identified).
- C.D. Bertram. The effects of wall thickness, axial strain and end proximity on the pressure area relation of collapsible tubes. *Journal of biomechanics*, 20(9):863-876, 1987 (An experimental study).
- C.D. Bertram. Dynamical system analyses of aperiodic flow-induced oscillations of a collapsible tube. *Journal de Physique Iii*, 5(12):2101-2116, 1995 (The paper briefly reviews dynamical systems analysis concepts and techniques applied to self-excited oscillation of flow through the collapsed flexible tubes).
- C.D. Bertram. Flow phenomena in floppy tubes. *Contemporary Physics*, 45(1):45-60, 2004.
- C.D. Bertram and R.J. Castles. Flow limitation in uniform thick-walled collapsible tubes. *Journal of Fluids and Structures*, 13(3):399-418, 1999.
- C.D. Bertram and W. Chen. Aqueous flow limitation in a tapered-stiffness collapsible tube. *Journal of Fluids and Structures*, 14(8):1195-1214, 2000.
- C.D. Bertram and N. S. J. Elliott. Flow-rate limitation in a uniform thin-walled collapsible tube, with comparison to a uniform thick-walled tube and a tube of tapering thickness. *Journal of Fluids and Structures*, 17(4):541-559, 2003.
- C.D. Bertram and S.A. Godbole. Lda measurements of velocities in a simulated collapsed tube. *Journal of Biomechanical Engineering-Transactions of the Asme*, 119(3):357-363, 1997 (Velocity measurements of flow in a perspex (plexiglas) tube which is locally deformed into an almost bi-lobar interior cross section).
- C.D. Bertram and T.J. Pedley. Steady and unsteady separation in an approximately two-dimensional indented channel. *Journal of Fluid Mechanics*, 130(MAY):315-345, 1983 (A experimental study on flow separations).
- C.D. Bertram and C.J. Raymond. Measurements of wave speed and compliance in a collapsible tube

during self-excited oscillations - a test of the choking hypothesis. *Medical & Biological Engineering & Computing*, 29(5):493-500, 1991 (An experimental study as the title suggests).

C.D. Bertram and C. Ribreau. Cross-sectional area measurement in collapsed tubes using the transformer principle. *Medical & Biological Engineering & Computing*, 27(4): 357-364, 1989 (An experimental measurements of collapsed tube areas).

C.D. Bertram and J. Tscherry. The onset of flow-rate limitation and flow-induced oscillations in collapsible tubes. *Journal of Fluids and Structures*, 22(8):1029-1045, 2006 (Experimental study on flow limitations).

C.D. Bertram, G.D. de Tuesta, and A.H. Nugent. Laser-doppler measurements of velocities just downstream of a collapsible tube during flow-induced oscillations. *Journal of Biomechanical Engineering-Transactions of the Asme*, 123(5):493-499, 2001 (Velocity measurements downstream of the collapsible tube).

B.S. Brook and T.J. Pedley. A model for time-dependent flow in (giraffe jugular) veins: uniform tube properties. *Journal of biomechanics*, 35(1):95-107, 2002 (A model for time-dependent flow in giraffe jugular veins).

Z.X. Cai and X. Y. Luo. A fluid-beam model for flow in a collapsible channel. *Journal of Fluids and Structures*, 17(1):125-146, 2003 (A steady collapsible channel flow model in which an elastic beam forms a part of the flexible channel).

C. Cancelli and T.J. Pedley. A separated-flow model for collapsible-tube oscillations. *Journal of Fluid Mechanics*, 157(AUG):375-404, 1985 (An analytical model which describes flow in collapsible tubes including the effects of the longitudinal wall tension and energy loss due to flow separation).

E.O. Carew and T.J. Pedley. An active membrane model for peristaltic pumping .1. periodic activation waves in an infinite tube. *Journal of Biomechanical Engineering-Transactions of the Asme*, 119(1):66-76, 1997 (A model for the coupled problem of wall deformation and fluid flow, based on thin-shell and lubrication theories, and driven by a propagating wave of smooth muscle activation, is proposed for peristaltic pumping in the ureter).

P.W. Carpenter and T.J. Pedley. Flow in collapsible tubes and past other highly compliant boundaries, chapter 2. flows in deformable tubes and channels. Theoretical models and biological applications (m. heil and oe jensen), 2003.

W.A. Conrad. Pressure-flow relationships in collapsible tubes. *Biomedical Engineering, IEEE Transactions on*, (4):284-295, 1969 (A classical paper on the pressure-flow characteristic of a short collapsible tube).

M.A. Crisfield. A fast incremental/iterative solution procedure that handles snap-through". *Computers and Structures*, 13(1-3):55-62, 1981 (A numerical method for post-bifurcation).

G.H. Dai, J.P. Gertler, and R. D. Kamm. The effects of external compression on venous blood flow and tissue deformation in the lower leg. *Journal of Biomechanical Engineering-Transactions of the Asme*, 121(6):557-564, 1999 (A two-dimensional FE study to determine venous collapse as a function of internal (venous) pressure and the external (surface) pressure) .

C.Davies and P.W. Carpenter. Instabilities in a plane channel flow between compliant walls. *Journal of Fluid Mechanics*, 352:205-243, 1997 (The interconnected behavior of flow-induced surface waves and Tollmien-Schlichting waves is examined both by direct numerical solution of the Orr-Sommerfeld equation and by means of an analytic shear layer theory).

D.Elad, R.D. Kamm, and A.H. Shapiro. Choking phenomena in a lung-like model. *Journal of Biomechanical Engineering-Transactions of the Asme*, 109(1):1-9, 1987 (A simple, continuous, one-dimensional model for the geometry and structure of the bronchial airways is used for the analysis of fluid flow patterns which have been observed in forced expiration maneuvers).

D.Elad, R.D. Kamm, and A.H. Shapiro. Steady compressible flow in collapsible tubes - application to forced expiration. *Journal of Fluid Mechanics*, 203:401-418, 1989 (Steady, one-dimensional flow of a compressible fluid through a collapsible tube is modeled, incorporating axial variations in the parameters of the conducting system, such as the tube unstressed cross-section area and wall stiffness, the external pressure and energy exchange with the environment).

N. Gavriely and J.B. Grotberg. Flow limitation and wheezes in a constant flow and volume lung preparation. *Journal of Applied Physiology*, 64(1):17, 1988 (An experimental study on flow limitation and wheezes using excised dog lungs).

N. Gavriely, J. Solway, A.S. Slutsky, R.D. Kamm, A.M. Shapiro, and J.M. Drazen. Effect of endotracheal-tube (ett) on co2 elimination (vco2) by small volume high-frequency ventilation (hfv) in dogs. *American Review of Respiratory Disease*, 125(4): 232-232, 1982.

N. Gavriely, Y. Palti, G. Alroy, and J.B. Grotberg. Measurement and theory of wheezing breath sounds. *Journal of Applied Physiology*, 57(2):481, 1984 (This work measured the time and frequency domain characteristics of breath sounds in seven asthmatic and three nonasthmatic wheezing patients. The power spectra of the wheezes were evaluated).

N. Gavriely, T.R. Shee, D.W. Cugell, and J.B. Grotberg. Flutter in flow-limited collapsible tubes: a mechanism for generation of wheezes. *Journal of Applied Physiology*, 66(5):2251, 1989 (This paper studies flutter in collapsible tubes as a possible mechanism for the generation of respiratory wheezes).

D.J. Griffiths. Flow of urine through the ureter: a collapsible, muscular tube undergoing peristalsis. *Journal of biomechanical engineering*, 111:206, 1989 (One-dimensional, lubrication-theory analysis shows that peristalsis can pump urine from kidney into the bladder only at relatively low mean rates of urine flow).

J.B. Grotberg and N. Gavriely. Flutter in collapsible tubes: a theoretical model of wheezes. *Journal of Applied Physiology*, 66(5):2262, 1989 (A mathematical analysis of flow through a flexible channel on flow-induced flutter oscillations that pertain to the production of wheezing breath sounds).

J.B. Grotberg and O.E. Jensen. Biofluid mechanics in flexible tubes. *Annual Review of Fluid Mechanics*, 36:121-147, 2004 (A review paper).

C. Guiot, P.G. Pianta, C. Cancelli, and T. J. Pedley. Prediction of coronary blood-flow with a numerical-model based on collapsible tube dynamics. *American Journal of Physiology*, 258(5):H1606-H1614, 1990 (A theoretical, hydrodynamic model of the vascular system feeding the left ventricle from which the inflow and outflow waveforms can be predicted given the waveforms of aortic and left ventricular pressure).

J.C. Guneratne and T. J. Pedley. High-reynolds-number steady flow in a collapsible channel. *Journal of Fluid Mechanics*, 569:151-184, 2006 (A two-dimensional model solved using high-Reynolds-number asymptotic methods, demonstrating a saddle-node bifurcation of the steady channel configuration).

A. L. Hazel and M. Heil. Steady finite-Reynolds-number flows in three-dimensional collapsible tubes. *Journal of Fluid Mechanics*, 486:79-103, 2003 (One of the earliest numerical simulations of the three-dimensional model of collapsible tube flows).

M. Heil. Stokes flow in collapsible tubes: computation and experiment 10. *Journal of Fluid Mechanics*, 353:285-312, 1997 (This paper studies the Stokes flow in collapsible tubes using both lubrication theory and full numerical simulations, and the results are compared with a corresponding experiment).

M. Heil and A.L. Hazel. Mass transfer from a finite strip near an oscillating stagnation point - implications for atherogenesis. *Journal of Engineering Mathematics*, 47(3-4): 315-334, 2003 (This paper studies the mass transfer from a finite-length strip near a two-dimensional, oscillating stagnation-point flow in an incompressible, Newtonian fluid).

M. Heil and T. J. Pedley. Large axisymmetrical deformation of a cylindrical-shell conveying a viscous-flow. *Journal of Fluids and Structures*, 9(3):237-256, 1995 (This paper examined the large axisymmetric deformations of collapsible tubes conveying a viscous flow using geometrically nonlinear Lagrangian shell theory to describe the deformation of the tube, and lubrication theory for the flow).

M. Heil and T. J. Pedley. Large post-buckling deformations of cylindrical shells conveying viscous flow. *Journal of Fluids and Structures*, 10(6):565-599, 1996 (This work paper examines the post-buckling deformations of cylindrical shells conveying viscous fluid).

M. Heil and S.L. Waters. Transverse flows in rapidly oscillating elastic cylindrical shells. *Journal of Fluid Mechanics*, 547:185-214, 2006 (This paper analyses the flows in fluid-conveying tubes whose elastic walls perform small-amplitude high-frequency oscillations using asymptotic methods as well as numerical simulations).

.M. Heil and S. L. Waters. How rapidly oscillating collapsible tubes extract energy from a viscous mean flow. *Journal of Fluid Mechanics*, 601(-1):199-227, 2008 (The work presents a combined theoretical and computational analysis of three-dimensional unsteady finite-Reynolds-number flows in collapsible tubes whose walls perform prescribed high-frequency oscillations. Results show that self-excited oscillations of collapsible tubes are much more likely to develop from steady-state configurations in which the tube is buckled non-axisymmetrically).

G.A. Holzapfel and R.W. Ogden. Modeling the layer-specific three-dimensional residual stresses in arteries, with an application to the human aorta. *Journal of the Royal Society Interface*, 7(46):787, 2010 (This paper provides the first analysis of the three-dimensional state of residual stress and stretch in an artery wall consisting of three layers (intima, media and adventitia), modeled as a circular cylindrical tube).

H. Huang, R. Virmani, H. Younis, A.P. Burke, R.D. Kamm, and R. T. Lee. The impact of calcification on the biomechanical stability of atherosclerotic plaques. *Circulation*, 103(8):1051-1056, 2001 (To test the hypothesis that calcification impacts biomechanical stresses in human atherosclerotic lesions, this paper studied 20 human coronary lesions with techniques that have previously been shown to predict plaque rupture locations accurately).

O.E. Jensen. Instabilities of flow in a collapsed tube. *Journal of Fluid Mechanics*, 220: 623-659, 1990 (This paper studies the effects of longitudinal wall tension and energy loss through flow separation on the stability of a one dimensional model.)

O.E. Jensen and M. Heil. High-frequency self-excited oscillations in a collapsible-channel flow. *Journal of Fluid Mechanics*, 481:235-268, 2003 (This paper presents a combined theoretical and computational analysis of three-dimensional unsteady finite-Reynolds-number flows in collapsible tubes, and establishes the critical Reynolds number,  $Recrit$ , at which the wall begins to extract energy from the flow).

O.E. Jensen and T.J. Pedley. The existence of steady flow in a collapsed tube. *Journal of Fluid Mechanics*, 206:339-374, 1989 (An analytical study on the existence of steady flows, which takes account of both longitudinal tension and jet energy loss Edownstream of the narrowest point).

R.D. Kamm and T.J. Pedley. Flow in collapsible tubes: a brief review. *Journal of biomechanical engineering*, 111:177, 1989 (A review paper).

R.D. Kamm and A. H. Shapiro. Unsteady-flow in a collapsible tube subjected to external-pressure or body forces. *Journal of Fluid Mechanics*, 95(NOV):1-78, 1979 (A one-dimensional, unsteady theory is developed for flows generated either by externally applied pressures or by body forces in thin-walled, collapsible tubes) .

F.P. Knowlton and E. H. Starling. The influence of variations in temperature and blood-pressure on the performance of the isolated mammalian heart. *The Journal of Physiology*, 44(3):206, 1912 (An experimental study).

K.Kounanis and D. S. Mathioulakis. Experimental flow study within a self oscillating collapsible tube. *Journal of fluids and structures*, 13(1):61-73, 1999 (The flow field within a self-excited flexible tube was studied by employing flow visualization, velocity and pressure measurements).

D.N. Ku. Blood flow in arteries. *Annual Review of Fluid Mechanics*, 29(1):399-434, 1997 (A classical review paper).

H. F. Liu, X.Y. Luo, Z.X. Cai, and T. J. Pedley. Sensitivity of unsteady collapsible channel flows to modeling assumptions. *Communications in Numerical Methods in Engineering*, 25(5), 2009 (A numerical study on show the unsteady collapsible channel flows change to different modeling assumptions of the elastic wall).

H.F. Liu, X. Y. Luo, and Z.X. Cai. Stability and energy budget of pressure-driven collapsible channel flows. *J. of Fluid Mechanics*, 705:348-370, 2012 (A numerical study on the energy budget of pressure-driven collapsible channel flows).

H.T. Low, Y.T. Chew, and C.W. Zhou. Pulmonary airway reopening: effects of non-newtonian fluid viscosity. *Journal of biomechanical engineering*, 119:298, 1997 (This numerical work considers the effects of non-Newtonian lining-fluid viscosity, particularly shear thinning and yield stress, on the reopening of the airways. The airway was simulated by a very thin, circular polyethylene tube, which

collapsed into a ribbon-like configuration.).

T. W. Lowe and T.J. Pedley. Computation of stokes flow in a channel with a collapsible segment. *Journal of fluids and structures*, 9(8):885-905, 1995 (The numerical solution of Stokes flow in two-dimensional channel in which a segment of one wall is formed by an elastic membrane under longitudinal tension and the remaining channel boundary is rigid is considered).

X. Luo, B. Calderhead, H. Liu, and W. Li. On the initial configurations of collapsible channel flow. *Computers and Structures*, 85(11-14):977-987, 2007 (This paper studies the plane strain and plane stress assumptions used in the elastic beam of the collapsible channel).

X. Y. Luo and T. J. Pedley. A numerical simulation of steady flow in a 2-d collapsible channel. *Journal of Fluids and Structures*, 9(2):149-174, 1995 (In this paper, steady flow in collapsible channel is simulated using FIDAP, and the results are compared with an analytical model).

X. Y. Luo and T. J. Pedley. A numerical simulation of unsteady flow in a 2-d collapsible channel. *J. Fluid Mech*, 314:191-225, 1996 (This paper uses an in-house ALE solver to reveal many self-excited oscillations that stem from the instabilities of the coupled system).

X. Y. Luo and T. J. Pedley. The effects of wall inertia on flow in a two-dimensional collapsible channel. *Journal of Fluid Mechanics*, 363:253-280, 1998 (This numerical study shows that when the wall inertia is included, there are flutter type self-excited oscillations in the system).

X. Y. Luo and T. J. Pedley. Multiple solutions and flow limitation in collapsible channel flows. *Journal of Fluid Mechanics*, 420:301-324, 2000 (Steady and unsteady numerical simulations are used to study the multiple solutions and flow limitation when the upstream transmural pressure is held constant).

X. Y. Luo, Z.X. Cai, W. G. Li, and T.J. Pedley. The cascade structure of linear instability in collapsible channel flows. *Journal of Fluid Mechanics*, 600:45-76, 2008 (This paper uses both the numerical and linear stability analyses to show that the system loses stability by passing through a cascade structure made of a succession of unstable zones, with mode number increasing as the wall stiffness is decreased).

A. Marzo, X.Y. Luo, and C.D. Bertram. Three-dimensional collapse and steady flow in thick-walled flexible tubes. *Journal of Fluids and Structures*, 20(6):817-835, 2005 (A numerical study on flows in thick-walled flexible tubes).

R.W. Ogden. Anisotropy and nonlinear elasticity in arterial wall mechanics. *Biomechanical modeling at the molecular, cellular and tissue levels*, pages 179-258, 2009 (This paper provides a theoretical framework based on the nonlinear theory of elasticity that can be used as the background against which the mechanical properties of soft biological tissue can be analysed by comparing theory with experimental data).

T.J. Pedley. The interaction between stirring and osmosis .1. *Journal of Fluid Mechanics*, 101(DEC):843-861, 1980 (An analytical description of the interaction between stirring and osmosis).

T. J. Pedley. Longitudinal tension variation in collapsible channels - a new mechanism for the breakdown of steady flow. *Journal of Biomechanical Engineering-Transactions of the Asme*, 114(1):60-67, 1992 (An analytical study on the effect of the longitudinal tension on of stability of the system).

T.J. Pedley and X.Y. Luo. Modeling flow and oscillations in collapsible tubes. *Theoretical and Computational Fluid Dynamics*, 10(1):277-294, 1998 (This paper outlines some of the models that have been developed to describe the standard experiment, of flow along a finite length of elastic tube mounted at its ends on rigid tubes and contained in a chamber whose pressure can be independently varied. Investigation of the streamlines of the flow and the distribution of viscous energy dissipation reveals how the one-dimensional model might be improved; but such improvement is as yet incomplete).

D. Pihler-Puzović and T.J. Pedley (2013). Stability of high-Reynolds-number flow in a collapsible channel. *Journal of Fluid Mechanics*, 714, pp 536-561 ( This is a study of high-Reynolds-number flow in a two-dimensional collapsible channel in the asymptotic limit of wall deformations confined to the viscous boundary layer. The system is modelled using interactive boundary-layer equations for a Newtonian incompressible fluid coupled to the freely moving elastic wall under constant tension and external pressure).

M.E. Ralph and T. J. Pedley. Flow in a channel with a moving indentation. *Journal of Fluid Mechanics*, 190:87-112, 1988 (The unsteady flow of a viscous, incompressible fluid in a channel with a moving

indentation in one wall has been studied by numerical solution of the Navier-Stokes equations).

M. P. Rast. Simultaneous solution of the Navier-Stokes and elastic membrane equations by a finite element method. *International Journal for Numerical Methods in Fluids*, 19 (12):1115-1135, 1994 (A finite element technique which solves the incompressible Navier-Stokes equations simultaneously with the elastic membrane equations on the flexible boundary. The elastic boundary position is parameterized in terms of distances along spines in a manner similar to that which has been used successfully in studies of viscous free surface flows).

E. Riks. An incremental approach to the solution of snapping and buckling problems\* 1. *International Journal of Solids and Structures*, 15(7):529-551, 1979 (This paper is concerned with numerical methods for computation of nonlinear equilibrium paths with continuation through limit points and bifurcation points).

A.H. Shapiro. Steady flow in collapsible tubes. *Journal of biomechanical engineering*, 99:126, 1977 (A classical paper in the field).

E.B. Shim and R.D. Kamm. Numerical simulation of steady flow in a compliant tube or channel with tapered wall thickness. *Journal of Fluids and Structures*, 16(8):1009-1027, 2002 (As the title suggests).

K.D. Stephanoff, T.J. Pedley, C.J. Lawrence, and T.W. Secomb. Fluid-flow along a channel with an asymmetric oscillating constriction. *Nature*, 305(5936):691-695, 1983. (Experimental results and theory on the flow of an incompressible fluid in a two-dimensional closed channel with an oscillating asymmetric constriction).

Stewart, P.S, Heil, M., S.L. Waters, and O.E. Jensen. Sloshing and slamming oscillations in collapsible channel flow. *Journal of Fluid Mechanics*, 662:288-319, 2010. (A simple model is used to demonstrate how fluid inertia in the downstream rigid channel segment, coupled to membrane curvature downstream of the moving constriction, together control slamming dynamics).

Stewart, P.S, Waters S.L. Jensen O.E.. Local and global instabilities of flow in a flexible-walled channel. *European Journal of Mechanics B/Fluids*, 28(4):541-557, 2009 (A 1-D model that shows how amplification of the primary global oscillatory instability can arise entirely from wave reflections with the rigid parts of the system, and how distinct mechanisms of energy transfer differentiate the primary global mode from other modes of oscillatory instability).

D. Tang, J. Yang, C. Yang, and D. N. Ku. A nonlinear axisymmetric model with fluid-wall interactions for steady viscous flow in stenotic elastic tubes. *Journal of biomechanical engineering*, 121:494, 1999 (A nonlinear axisymmetric model with fluid-wall interactions is introduced to simulate the viscous flow in a compliant stenotic tube using ADINA).

O.R. Tutty and T. J. Pedley. Oscillatory flow in a stepped channel. *Journal of Fluid Mechanics*, 247:179-204, 1993 (Two-dimensional, unsteady flow of a viscous, incompressible fluid in a stepped channel has been studied by the numerical solution of the Navier-Stokes equation using an accurate finite-difference method).

H.M. Wang, H. Gao, X.Y. Luo, C. Berry, B.E. Griffith, R.W. Ogden, and T.J. Wang. Structure-based finite strain modeling of the human left ventricle in diastole, *International Journal for Numerical Methods in Biomedical Engineering*, 29, 83-103, 2013 (A three-dimensional computational model of the human left ventricle is developed from non-invasive imaging data, a rule-based fibre structure, and a structure-based constitutive model. The sensitivity of the constitutive parameters and fibre distributions is studied).

H.M. Wang, X.Y. Luo, H. Gao, R.W. Ogden, B.E. Griffith, C. Berry, and T.J. Wang. A Modified Holzapfel-Ogden Law for a Residually Stressed Finite Strain Model of the Human Left Ventricle in Diastole, *Biomechanics and Modeling in Mechanobiology*, 13, 99-113, 2014 (This work introduces a modified Holzapfel-Ogden hyperelastic constitutive model for ventricular myocardium that accounts for residual stresses. The effects of residual stresses are then investigated using a MRI-derived model of the human left ventricle in diastole).

R.J. Whittaker, S.L. Waters, O. E. Jensen, J. Boyle, and M. Heil. The energetics of flow through a rapidly oscillating tube. part 1. general theory. *J. Fluid Mech*, 648:83-121, 2010a (This paper examines the effect of prescribed wall-driven oscillations of a flexible tube of arbitrary cross-section, through which a flow is driven by prescribing either a steady flux at the downstream end or a steady pressure difference between the ends. General asymptotic results are derived).

R.J. Whittaker, M. Heil, J. Boyle, O.E. Jensen, and S. L. Waters. The energetics of flow through a rapidly oscillating tube. part 2. application to an elliptical tube. *J. Fluid Mech*, 648:123-153, 2010b (Continues with part I, this work illustrates how these asymptotic results can be applied to the case of flow through a finite-length axially non-uniform tube of elliptical cross-section – a model of flow in a Starling resistor).

R. J. Whittaker, M. Heil, O. E. Jensen, and S. L. Waters. Predicting the onset of high-frequency self-excited oscillations in elastic-walled tubes. *Proceedings of the Royal Society A: Mathematical, Physical and Engineering Science*, 466(2124):3635, 2010c (This paper presents a theoretical description of flow-induced self-excited oscillations in the Starling resistor. The authors derive a one-dimensional eigenvalue problem for the frequencies and mode shapes of the oscillations, and determine the slow growth or decay of the normal modes by considering the system's energy budget).

R. J. Whittaker, M. Heil, O. E. Jensen, and S. L. Waters. A rational derivation of a tube law from shell theory. *The Quarterly Journal of Mechanics and Applied Mathematics*, 63(4):465, 2010d (As the title suggests).

R. J. Whittaker, A shear-relaxation boundary layer near the pinned ends of a buckled elastic-walled tube, 80(6), 1932-1967, *IMA Journal of Applied Mathematics* (This paper derived a boundary-layer model for the deformations near an end of a thin-walled elastic tube that is pinned to a rigid elliptical support).

R. Wild, T. J. Pedley, and D. S. Riley. Viscous-flow in collapsible tubes of slowly varying elliptical cross-section. *Journal of Fluid Mechanics*, 81(JUN24):273-294, 1977 (Lubrication theory is used in this work to calculate the velocity and pressure distribution in an elliptical collapsible tube whose cross-sectional area and eccentricity vary slowly and in a given way with longitudinal distance  $x$ ).

Feng Xu, John Billingham, and Oliver E Jensen. Divergence-driven oscillations in a flexible-channel flow with fixed upstream flux. *Journal of Fluid Mechanics*, 723:706 – 733, 2013. (Demonstrated that mode-2 instability of flux-driven system can be driven by divergence of two different modes)

Feng Xu, John Billingham, and Oliver E Jensen. Resonance-driven oscillations in a flexible-channel flow with fixed upstream flux and a long downstream rigid segment. *Journal of Fluid Mechanics*, 746:368–404, 2014. (This papers shows that a mode-2 instability of flux-driven system can be induced by a 1:1 resonant interaction as a result of a long downstream rigid segment)

N. Yamaki, 1984. *Elastic Stability of Circular Cylindrical Shells*. North-Holland, Amsterdam (A classical book on elastic stability of cylindrical Shells).

Y. Zhu, X. Y. Luo, and R. W. Ogden. Asymmetric bifurcations of thick-walled circular cylindrical elastic tubes under axial loading and external pressure. *International Journal of Solids and Structures*, 45(11-12):3410-3429, 2008 (This paper considers bifurcation of a thick-walled circular cylindrical tube, and studies the effects of wall thickness and the ratio of length to radius on the bifurcation behavior).

Y. Zhu, X. Y. Luo, and R. W. Ogden. Nonlinear axisymmetric deformations of an elastic tube under external pressure. *European Journal of Mechanics-A/Solids*, 29(2):216-229, 2010 (The problem of the finite axisymmetric deformation of a thick-walled circular cylindrical elastic tube under external pressure is formulated for an incompressible isotropic neo-Hookean material. Typical nonlinear characteristics exhibited are the “corner bulging” of short tubes, and multiple modes of deformation for longer tubes).

Y. Zhu, X. Y. Luo, H. M. Wang, R. W. Ogden, and Colin B. Nonlinear buckling of three-dimensional thick-walled elastic tubes under pressure. *International Journal of Non-Linear Mechanics*, 48:1-14, 2013 (This paper carries out a fully nonlinear approach for the post-buckling solutions of Neo-Hookean thick-walled tubes under external pressure).

### Biographical Sketches

**Xiaoyu Luo** received her first degree in Theoretical Solid Mechanics at Xi'an Jiaotong University, China, where she also completed her MSc and PhD in Fluid Mechanics and Biomechanics. She has been working in the UK since 1992 and became a Professor of Applied Mathematics at the University of Glasgow in 2008. Her main research interests are in fluid-structure interaction and soft tissue mechanics, with applications to modeling of heart, heart valves, artery, gallbladders and several other physiological problems. She has published over 70 papers in the international journals. She is a fellow of Royal Society of Edinburgh, IMechE, member of the EPSRC college, a conjunct Professor of Xi'an Jiaotong University and Northwest Polytechnic University, China, and in the editorial boards of four international journals.